

A simplified human birth model: translation of a rigid cylinder through a passive elastic tube

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Work supported in part by NSF DMS 1043626

Motivation

Vaginal delivery is linked to

- \triangleright shorter post-birth hospital stays
- \blacktriangleright lower likelihood of intensive care stays
- \blacktriangleright lower mortality rates [1]

Fluid mechanics greatly informs the total mechanics of birth.

- \blacktriangleright vernix caseosa
- \blacktriangleright amniotic fluid

[1] C. S. Buhimschi, J. A. Buhimschi (2006). Advantages of vaginal delivery. Clinical obstetrics and gynecology. Fig. 1: "HumanNewborn" by Ernest F - Own work. Licensed under CC BY-SA 3.0 via Commons - [https://](https://commons.wikimedia.org/wiki/File:HumanNewborn.JPG#/media/File:HumanNewborn.JPG) commons.wikimedia.org/wiki/File:HumanNewborn.JPG#/media/File:HumanNewborn.JPG Fig. 2: "Postpartum baby2" by Tom Adriaenssen - <http://www.flickr.com/photos/inferis/110652572/>. Licensed under CC BY-SA 2.0 via Commons - [https://commons.wikimedia.org/wiki/File:Postpartum_baby2.](https://commons.wikimedia.org/wiki/File:Postpartum_baby2.jpg#/media/File:Postpartum_baby2.jpg) [jpg#/media/File:Postpartum_baby2.jpg](https://commons.wikimedia.org/wiki/File:Postpartum_baby2.jpg#/media/File:Postpartum_baby2.jpg)

Physical Experiment

- \triangleright Rigid acrylic cylinder (fetus)
- \blacktriangleright Passive elastic latex tube (birth canal)
- \triangleright Viscous fluid methyl cellulose and water (amniotic fluid)
- \triangleright Rigid cylinder is pulled through center of elastic tube at constant velocity

Numerical Model

time $t = 0.0000 s$

The Model: Solid Behavior

- \blacktriangleright Tube modeled by network of Hookean springs.
- Force at point x_i due to spring from point x_m : $\mathsf{f}(\mathsf{x}_l) = \tau \left(\frac{\|\mathsf{x}_m - \mathsf{x}_l\|}{\Delta_{lm}} - 1 \right) \frac{(\mathsf{x}_m - \mathsf{x}_l)}{\|\mathsf{x}_m - \mathsf{x}_l\|}$ \blacktriangleright τ chosen to match elastic
	- properties to physical experiment. [2]

 \blacktriangleright A constant velocity **u** is specified in the z-direction.

[2] H. Nguyen and L. Fauci (2014). Hydrodynamics of diatom chains and semiflexible fibres, J. R. Soc. Interface.

The Model: Fluid Dynamics

Fluid Behavior is governed by the Stokes equations, with regularized forces at K discrete points in the system:

$$
0=-\nabla p+\mu\Delta \mathbf{u}+\sum_{k=0}^K\mathbf{f}_k\phi_{\varepsilon}(\mathbf{x}-\mathbf{x}_k),\nabla\cdot\mathbf{u}=0,
$$

which have solution [3],[4]

$$
\mathbf{u}(\mathbf{x}) = \frac{1}{\mu} \sum_{k=1}^{K} \left[(\mathbf{f}_k \cdot \nabla) \nabla B_{\varepsilon}(|\mathbf{x} - \mathbf{x}_k|) - \mathbf{f}_k G_{\varepsilon}(|\mathbf{x} - \mathbf{x}_k|) \right],
$$

$$
\rho(\mathbf{x}) = \sum_{k=1}^{K} \left[\mathbf{f}_k \cdot \nabla G_{\varepsilon}(|\mathbf{x} - \mathbf{x}_k|) \right],
$$

where $\Delta B_\varepsilon = \mathcal{G}_\varepsilon, \Delta \mathcal{G}_\varepsilon = \phi_\varepsilon(r) = \frac{15\varepsilon^4}{8\pi (r^2 + \varepsilon^2)}$ $\frac{15\varepsilon}{8\pi(r^2+\varepsilon^2)^{(7/2)}}$.

Here, μ is viscosity, \mathbf{x}_k are points on discretized tube and rod, \mathbf{f}_k is the force at that point, and ε is a regularization parameter.

[3] R. Cortez (2001). Method of Regularized Stokeslets, SIAM Journal of Scientific Computing. [4] R. Cortez, L. Fauci, A. Medovikov (2005). The method of regularized Stokeslets in three dimensions: analysis, validation, and application to helical swimming, Physics of Fluids.

Using the solution to the regularized Stokes equations for a given regularization function ϕ_{ε} :

- (1) Calculate spring forces in the tube based on its deformation, and calculate the velocity they induce on the inner cylinder.
- (2) Solve for additional forces necessary on inner cylinder points to achieve its desired constant velocity.
- (3) Evaluate the velocity points on tube and inner cylinder. (Velocity and pressure can be evaluated at any other point in the system.)
- (4) Update the tube and rod positions using these velocities one step forward in time.
- (5) Repeat.

Validation: Velocity Profile Between Cylinder and Solid Tube

Figure: The velocity profile between an infinitely long rigid cylinder of radius R_c and an infinitely long rigid tube of radius R_t is $u(r) = \frac{U(\ln(R_t) - \ln(r))}{\ln(R_t) - \ln(R_c)}$. This is compared with the velocity computed using the method of regularized stokeslets with varying values for ε .

Results: System Behavior and Elastic Buckling

time $t = 0.0000 s$

Results: System Behavior and Elastic Buckling

time $t = 0.0000 s$

Source man

Results: Causes of Elastic Buckling

 $time = 0.0000 seconds$

Results: Force on Rigid Cylinder

- \blacktriangleright In blue: Drag force on rigid inner cylinder as it moves at constant velocity through elastic tube
- \blacktriangleright In red: Asymptotic approximation to the drag force on a long, slender cylinder moving along its axis through a viscous fluid [5]: $\mathsf{F} = \frac{4\pi\mu UL}{2\ln(L/r)-1}$

[5] C. Pozrikidis (2011). Introduction to theoretical and computational fluid dynamics, Oxford University Press.

Results: Force Variation with Diameter and Velocity

- \blacktriangleright Force doubles when velocity doubles, as expected in Stokes flow regime
- \blacktriangleright Force decreases as diameter of inner cylinder decreases

Future Work

 \blacktriangleright Further analysis of tube buckling behavior

- \triangleright Variation of diameter and length of rigid cylinder and tube
- \triangleright Variation of velocity of rigid cylinder
- \triangleright Variation of elasticity of tube
- \blacktriangleright Increase realism
	- \triangleright active elastic tube / modeling peristalsis
	- \blacktriangleright more accurate geometry

Slides available at <math.tulane.edu/~rpealate>